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FULL PAPER

The use of texture-based radiomics CT analysis to predict outcomes in early-stage non-small cell lung cancer treated with stereotactic ablative radiotherapy

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Objective: Stereotactic ablative radiotherapy (SABR) is being increasingly used as a non-invasive treatment for early-stage non-small cell lung cancer (NSCLC). A non-invasive method to estimate treatment outcomes in these patients would be valuable, especially since access to tissue specimens is often difficult in these cases.

Methods: We developed a method to predict survival following SABR in NSCLC patients using analysis of quantitative image features on pre-treatment CT images. We developed a Cox Lasso model based on two-dimensional Riesz wavelet quantitative texture features on CT scans with the goal of separating patients based on survival.

Results: The median log-rank p -value for 1000 cross-validations was 0.030. Our model was able to separate patients based upon predicted survival. When we added tumor size into the model, the p -value lost its significance, demonstrating that tumor size is not a key feature in the model but rather decreases significance likely due to the relatively small number of events in the dataset.

Furthermore, running the model using Riesz features extracted either from the solid component of the tumor or from the ground glass opacity (GGO) component of the tumor maintained statistical significance. However, the p -value improved when combining features from the solid and the GGO components, demonstrating that there are important data that can be extracted from the entire tumor.

Conclusions: The model predicting patient survival following SABR in NSCLC may be useful in future studies by enabling prediction of survival-based outcomes using radiomics features in CT images.

Advances in knowledge: Quantitative image features from NSCLC nodules on CT images have been found to significantly separate patient populations based on overall survival ($p = 0.04$). In the long term, a non-invasive method to estimate treatment outcomes in patients undergoing SABR would be valuable, especially since access to tissue specimens is often difficult in these cases.

INTRODUCTION

Staging of lung cancer with pathologic tissue has long been the gold-standard to predict recurrence risk in non-small cell lung cancer (NSCLC). When surgery is pursued,

patients are often upstaged due to the discovery of occult nodal metastasis.¹⁻³ However, medical comorbidities of patients often limit access to pathologic tissues and surgical management. As an alternative to surgery, non-invasive

stereotactic ablative radiation therapy (SABR) is increasingly chosen for both definitive and palliative treatment in early-stage patients and has been linked to improved survival in elderly lung cancer patients.^{4,5} Often SABR and other non-invasive treatments such as conventional radiation, targeted therapy and chemotherapy render surgical staging of the cancer excessive; instead, cancer may be staged by radiological imaging techniques with limited sensitivity and specificity.⁶ For these reasons, image-based biomarkers could play an important role in guiding the treatment of NSCLC patients who are high-risk candidates for invasive procedures and surgery.

Early-stage NSCLC is often curable. For patients who are poor surgical candidates or who refuse surgery, SABR is an alternative treatment with excellent outcomes, highlighted by the Radiation Therapy Oncology Group (RTOG) 0236 clinical trial⁷ and multiple single and multiinstitutional experiences.^{8–10} Although SABR treatment can result in greater than 90% local control, there is a need for methods that can predict which patients are at highest risk of regional or distant metastasis and who may benefit from upfront systemic treatment. Semantic (human-determined) imaging-based biomarkers have recently been described for Stage 1 NSCLC treated with SABR, such as tumor size, contact to mediastinal pleura, and the maximum standard uptake value (SUV) in positron emission tomography (PET).¹¹ In this study, we hypothesized that quantitative (machine-calculated) image based features from pre-treatment CT scans can predict the risk for tumor recurrence.

Image-based quantitative features from pre-treatment imaging may have the power to predict short-term treatment success and long-term outcomes. Quantitative image features, particularly those based on lesion heterogeneity, have had success in predicting outcomes for a wide range of cancers,^{12–15} including response to chemotherapy,^{16,17} long-term survival in lung cancer,¹⁸ and long-term survival in other cancers.^{19,20}

Our approach uses a quantitative model derived from two-dimensional (2D) Riesz wavelet analysis.²¹ We employed a Cox Lasso model to develop the model, we successfully predicted survival on an expanded cohort of patients, the results were not dependent on tumor size being factored into the model, and we found that both the solid and ground glass opacity (GGO) components provide predictive Riesz data. Our results contribute to the growing literature of radiomics analysis of patient images, which in the context of stereotactic radiation can serve as a methodology to predict outcomes for patients with early-stage NSCLC to guide treatment decisions for patients treated non-invasively.

METHODS AND MATERIALS

Patient cohort

A cohort of 116 patients was assembled retrospectively with institutional review board approval from patients treated with thoracic SABR for biopsy-confirmed, primary NSCLC, at Stanford University. We chose the patients based upon a follow-up window described in the methods at our institution. We included all of the patients that met the criteria described where we had the appropriate imaging and contours readily available. A superset

of 110 patients of this cohort has been previously described.¹¹ This prior article dealt with identifying manually extracted imaging-based predictors of disease progression whereas in this manuscript we used quantitative features to separate patient populations based on overall survival. Only patients with available radiation planning CT images were included. All cancers were Stage I by the seventh edition AJCC staging manual.²² Most patients received SABR rather than surgery because of surgical risk due to comorbid conditions, but some refused surgery. Patients were not included if they received chemotherapy prior to a diagnosis of metastatic failure, if they had synchronous tumors, or if they had received a new diagnosis of primary NSCLC following SABR. Patients were also excluded if they had been previously treated for NSCLC, unless it was for prior Stage I disease treated exclusively with lobectomy or pneumonectomy at least 1 year prior to SABR and the second tumor was considered to be a new primary tumor by the treating physicians. SABR treatment dose was determined via a tumor volume-adapted SABR dosing strategy.²³ All patient images were deidentified prior to analysis, so no informed consent was required from participants.

Patient treatments and outcomes

For each patient, after the decision was made to undergo SABR treatment, patients received a treatment planning CT or PET/CT in the radiation oncology department and typically started treatment within 1 to 2 weeks. Depending upon the clinical and imaging features of the tumor, an appropriate radiation dose was chosen. Patients were treated with a tumor volume-adapted fractionation strategy, with the majority of doses exceeding a BED 100, as described in Shultz et al.¹¹ Table 1 describes the patient population, clinical factors, and treatment dose fractionation schemes. Patients were followed with CT and/or PET/CT imaging every 3 months after treatment. Of 116 patients there were a total of 52 events including 12 local failures, 20 regional failures, 18 distant failures and 39 deaths (Table 2).

CT imaging

CT-images, acquired at a single institution using a General Electric CT scanner, were without contrast and were used for treatment planning. Of the 116 patients, 69% ($n = 80$) of CT scans had 1.25 mm slice thickness and 20% ($n = 23$) had 2.5 mm slice thickness. Most patient CT scans (78%, $n = 90$) had in-plane pixel spacing of 0.98 mm; pixel spacing varied in other patients from 0.80 to 1.37 mm.

Outcomes and follow-up

Assessed outcomes included local failure with tumor recurrence in the same lobe of the treated tumor, regional failure with recurrence in regional lymph nodes or the same hemithorax, distant failure consisting of metastatic disease, distant failure without regional failure, progression-free survival and overall survival. Survival outcomes were determined objectively. Local, regional, and distant recurrence was determined using a combination of new findings on imaging, serial progression on imaging, and in many cases confirmed with a biopsy. If progression was convincing based upon the clinical picture treatment was often initiated without a biopsy. Imaging included diagnostic

Table 1. Patient characteristics

Variables	Number of patients (%)
Age (years): median 77, range 42–92	
<60	11 (9)
60–69	26 (22)
70–79	42 (36)
80–89	32 (28)
90+	5 (4)
Gender	
Male	53 (46)
Female	63 (58)
Site	
Right upper lobe	37 (31)
Right middle lobe	1 (1)
Right lower lobe	21 (18)
Left upper lobe	26 (22)
Left lower lobe	31 (26)
Histology	
Adenocarcinoma	70 (60)
Squamous cell carcinoma	31 (27)
NSCLC- unspecified	14 (12)
Atypia	1 (1)
Stage	
IA	85 (73)
IB	31 (27)
Dose/Fractions/BED₁₀ acute	
25/1/87.5	33 (28)
30/1/120	6 (5)
34/1/149.6	1 (1)
40/4/80	12 (10)
48/4/105.6	1 (1)
50/4/112.5	35 (30)
50/5/100	3 (3)
54/3/151.2	4 (3)
60/3/180	19 (16)
60/5/132	2 (2)
Karnofsky performance status	
≥90	28 (24)
80	35 (30)
70	38 (33)
<70	15 (13)

BED, biologically effective dose; NSCLC, non-small cell lung cancer;

CT scans, PET scans, and often both were utilized to improve diagnostic assessment. Clinical exam and/or interval imaging was performed at each follow-up evaluation. All follow-up

Table 2. Patient outcomes

Patterns of failure	Number of patients (%)	Median time of (range of) failures (m)
LF	12 (10)	11 (1–39)
RF	20 (17)	8 (1–52)
DF	18 (16)	13.5 (1–48)
DF-(RF + LF)		9.5 (1–48)
Survival characteristics		Median time of (range of) survival (m)
OS	77 (66)	18 (2–62)
PFS	64 (55)	17 (2–62)

DF, distant failure; DF-(RF+LF), distant failure without regional failure; LF, Local failure; OS, overall survival; PFS, progression-free survival; RF, regional failure;

evaluations included imaging that corroborated each clinical outcome, but clinical exam was not performed for some patients who were followed by their local physician. Minimum, median and maximum follow-up time for the entire cohort was 2, 18.5 and 66 months.

Quantitative features

We assessed the tumors using a three-dimensional region of interest (ROI) that captures the gross tumor volume that was delineated by the treating physician. We chose a single 2D slice on which to extract quantitative imaging features; this slice was the largest 2D ROI that did not contain any pixel with HU > 3000 (to exclude artifacts from fiducial marker placement). Median 2D ROI bounding box size was 20 × 20 pixels.

Multiple techniques, involving Gaussian image filtering and Riesz wavelets (low-pass or high pass),^{24–26} were used to extract quantitative features to capture lesion texture. Features were extracted from the solid center, the rim or the full tumor (Figure 1). Depending on the parameters used, the number of features extracted from a single 2D ROI bounding box varied between 2 and 30 quantitative values. Features were used with or without nodule size to test it as a confounding factor.

More technical information regarding Riesz wavelet analysis can be found in [Supplementary Material 1](#).

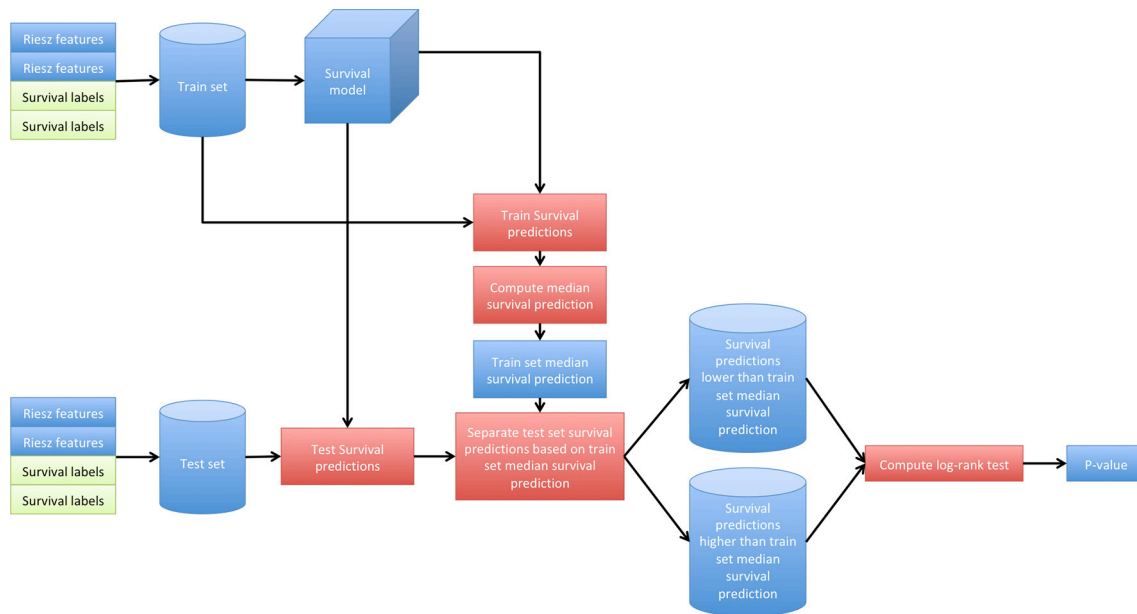
Statistical analysis

For predictive model selection, we used the Cox proportional-hazards Lasso method.²³ Based on the model's predictions, patients were partitioned into two exclusive groups, which were

Figure 1. Full GTV, GGO, solid center. GGO, ground glass opacity; GTV, gross tumor volume.



Figure 2. Survival cross-validation process.



then compared with the use of a log-rank test.²⁷ A low log-rank p -value ($p < 0.05$) indicated effectiveness at separating the data into cohorts with significantly different prognoses. For visualizing differences in prognosis between separated cohorts, we used Kaplan-Meier charts.²⁸

More technical information regarding Cox Lasso method and statistical analysis can be found in [Supplementary Material 1](#).

Cross-validated predictive model

During cross-validation, we randomly separated 58 patients for model fitting and 58 patients for testing (Figure 2). The goal of the analysis was to train a predictive model on the 58 model fitting patients and to separate the 58 testing patients, using the predictive model, into two groups with significantly different survival curves ($p < 0.05$). The process was performed 1000 times and the median p -value was selected as the final result.

More technical information regarding cross-validation method can be found in [Supplementary material](#).

RESULTS

Cross-validated predictive modeling

For this study, we were most interested in the ability of the model to predict overall survival given the number of events. However, predicting many types of treatment failures could be important from a clinical perspective, and each could have a distinct biologic rationale. For example, factors that impact local and distant failure could be very different and could have different texture features. Given our interest in different types of treatment failures, we assessed outcomes that included local failure, regional failure, distant failure, distant failure without regional failure, progression-free survival and overall survival.

Survival results are median 1000 cross-validation p -values. Significant results ($p < 0.05$) were found when using overall survival outcomes but no other outcomes (Table 3).

In addition to the above findings, we observed that the use of Gaussian filtering and high-pass Riesz wavelets on full tumor

Table 3. Significant analyses and input parameters for measurement

Outcomes	Nodule size	Features	Filtering	Riesz parameters	p -value
Overall survival	Without	Full nodule	Gaussian	High-pass, $N = 1$, $J = 1$	0.04
Overall survival	Without	Solid center	Gaussian	High-pass, $N = 2$, $J = 3$	0.03
Overall survival	Without	Solid center	Gaussian	High-pass, $N = 4$, $J = 1-3$	0.04
Overall survival	Without	Solid center	Without	High-pass, $N = 2$, $J = 3$	0.04
Overall survival	Without	Solid center	Without	High-pass, $N = 2$, $J = 3$	0.04
Overall survival	Without	GGO	Gaussian	High-pass, $N = 2$, $J = 2,4$	0.04
Overall survival	Without	Solid center and GGO	Gaussian	High-pass, $N = 2$, $J = 3$	0.04
Overall survival	Without	Solid center and GGO	Without	High-pass, $N = 1$, $J = 3$	0.04

GGo, ground glass opacity;

nodule without nodule size was significant or nearly significant for outcomes such as overall survival ($p = 0.04-0.07$), progression-free survival ($p = 0.06-0.09$) and distant failure without regional failure ($p = 0.09-0.14$). This confirms that filtering and high-pass Riesz result in separating the data the greatest and that nodule size confounds the model that may be due to the variation in nodule size and the relatively low overall sample size.

A pattern that was statistically significant ($p = 0.05$) or nearly significant ($p < 0.10$) was observed with the use of Gaussian filtering, high-pass Riesz wavelets, without nodule size feature included in the model for outcomes such as overall survival, progression-free survival and distant failure without regional failure.

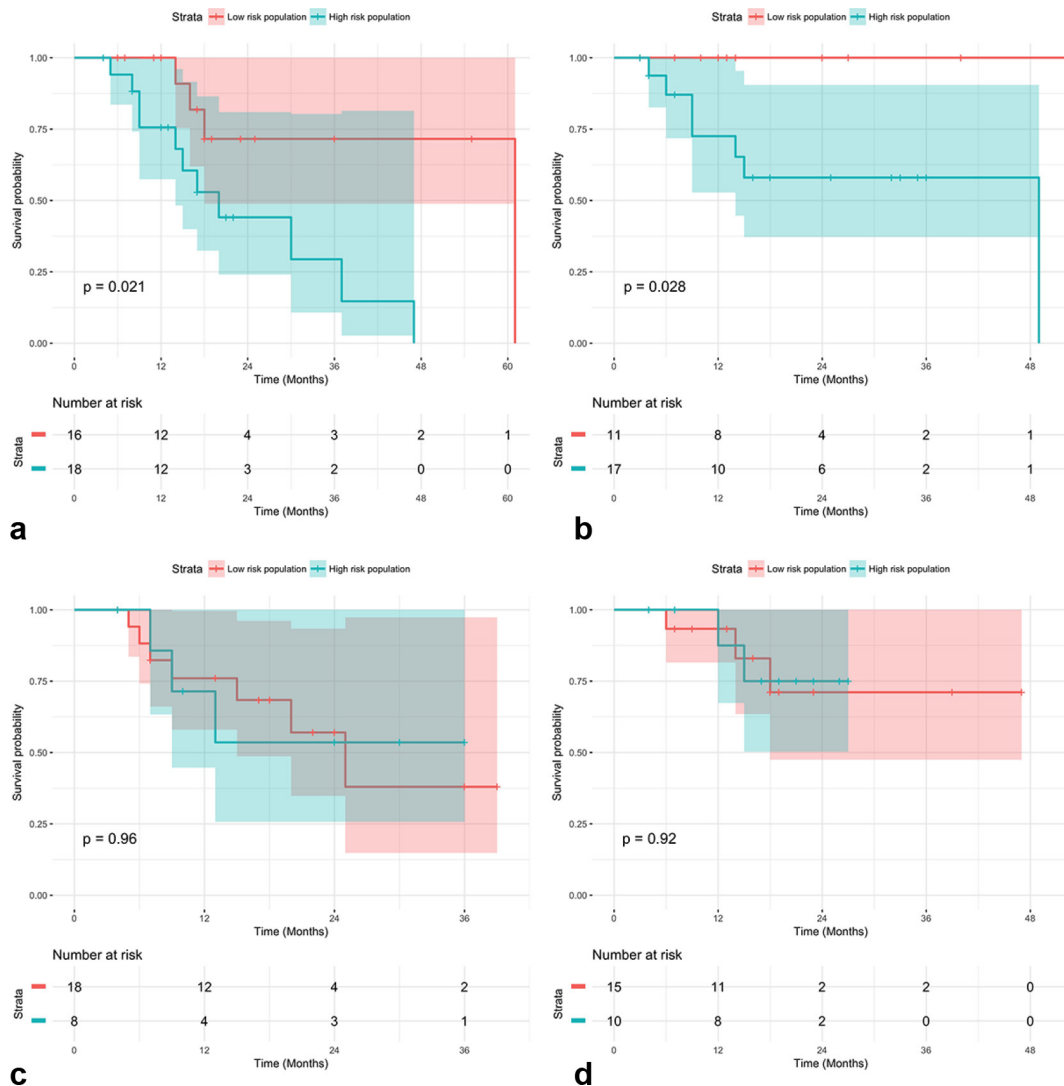
Kaplan–Meyer charts show examples of statistically significant (Figure 3A,B) and non-significant (Figure 3C,D) results

generated with the use of our cross-validated predictive model.

DISCUSSION

Quantitative image analysis provides useful information to evaluate disease and guide treatment decisions based upon assessed risks. In this study, we investigated the association of treatment failure with quantitative features based on Riesz wavelets that represent lesion texture. Features of this form have been shown in prior work to correlate with tumor type, progression and response to therapy. Our quantitative features show statistically significant results in separating patients with early-stage NSCLC into groups of different survival. Other interesting results that need further investigations have been found during cross-validation in outcomes such as overall survival, progression-free survival and distant failure without regional failure.

Figure 3.(A) Kaplan–Meyer chart ($p = 0.021$) evaluating progression-free survival, full nodule, with Gaussian filtering, high-pass Riesz wavelets ($N = 1, J = 1$) (B) Kaplan–Meyer chart ($p = 0.028$) evaluating distant failure, full nodule, with Gaussian filtering, high-pass Riesz wavelets ($N = 1, J = 1$) (C) Kaplan–Meyer chart ($p = 0.96$) showing lack of significance for progression-free survival, full nodule, with Gaussian filtering, high-pass Riesz wavelets ($N = 1, J = 1$) (D) Kaplan–Meyer chart ($p = 0.92$) showing lack of significance for distant failure, full nodule, with Gaussian filtering, high-pass Riesz wavelets ($N = 1, J = 1$).



We believe that our approach has great potential to predict the biologic nature of cancers thereby distinguishing risk for local, regional, and distant failure. Our method is also thought to be generalizable, and will be applying it to additional malignancies. A limitation of our study is the limited number of events in our data set, which could hinder our ability to develop a robust model. In addition, we recognize that the size of our patient population is limited, though we included all patient data available at our institution that met inclusion criteria. The goal of our analysis was to develop the model and explore its potential clinical value. Exploring larger data sets will be needed to validate the predictive capability of our models, and we are actively pursuing larger validation sets. Such analysis may also be able to understand the relative importance of the solid and GGO components of a tumor for their clinical and biological significance. Nevertheless, our current results appear promising.

In addition to evaluating larger data sets, our future work will be to assess the potential clinical benefit of implementing this methodology in prospective clinical settings and to incorporate more sophisticated analyses. Additional modeling could include three-dimensional image features, which have been shown to be

more effective at predicting malignancy in breast lesions than 2D features.²⁴

All analyses were performed on treatment planning CT scans with the aim of decreasing variability. However, slice thickness, the timing of contrast, and level of breath-hold was not consistent throughout the years of treatment, so this variation could limit our results. Standardization using pretreatment diagnostic thoracic CT scans may have a positive impact on future results.

The quantitative techniques employed here are novel and worth considering in future analyses that involve quantitative features as predictors of longitudinal censored outcomes. Particularly, our use of Cox Proportional Hazards Lasso regression is a powerful method of determining which quantitative features would be viable predictors of survival in future cohorts.

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REFERENCES

- Asamura H, Goya T, Koshiishi Y, Sohara Y, Eguchi K, Mori M, et al. A Japanese lung cancer registry study: prognosis of 13,010 resected lung cancers. *J Thorac Oncol* 2008; **3**: 46–52. doi: <https://doi.org/10.1097/JTO.0b013e31815e8577>
- Licht PB, Jørgensen OD, Ladegaard L, Jakobsen E. A national study of nodal upstaging after thoracoscopic versus open lobectomy for clinical stage I lung cancer. *Ann Thorac Surg* 2013; **96**: 943–50. doi: <https://doi.org/10.1016/j.athoracsur.2013.04.011>
- Boffa DJ, Kosinski AS, Paul S, Mitchell JD, Onaitis M. Lymph node evaluation by open or video-assisted approaches in 11,500 anatomic lung cancer resections. *Ann Thorac Surg* 2012; **94**: 347–53. doi: <https://doi.org/10.1016/j.athoracsur.2012.04.059>
- Chang JY, Senan S, Paul MA, Mehran RJ, Louie AV, Balter P, et al. Stereotactic ablative radiotherapy versus lobectomy for operable stage I non-small-cell lung cancer: a pooled analysis of two randomised trials. *Lancet Oncol* 2015; **16**: 630–7. doi: [https://doi.org/10.1016/S1470-2045\(15\)70168-3](https://doi.org/10.1016/S1470-2045(15)70168-3)
- Palma D, Visser O, Lagerwaard FJ, Belderbos J, Slotman BJ, Senan S. Impact of introducing stereotactic lung radiotherapy for elderly patients with stage I non-small-cell lung cancer: a population-based time-trend analysis. *J Clin Oncol* 2010; **28**: 5153–9. doi: <https://doi.org/10.1200/JCO.2010.30.0731>
- Gould MK, Kushner WG, Rydzak CE, Maclean CC, Demas AN, Shigemitsu H, et al. Test performance of positron emission tomography and computed tomography for mediastinal staging in patients with non-small-cell lung cancer: a meta-analysis. *Ann Intern Med* 2003; **139**: 879–92. doi: <https://doi.org/10.7326/0003-4819-139-11-200311180-00013>
- Timmerman R, Paulus R, Galvin J, Michalski J, Straube W, Bradley J, et al. Stereotactic body radiation therapy for inoperable early stage lung cancer. *JAMA* 2010; **303**: 1070–6. doi: <https://doi.org/10.1001/jama.2010.261>
- Shibamoto Y, Hashizume C, Baba F, Ayakawa S, Manabe Y, Nagai A, et al. Stereotactic body radiotherapy using a radiobiology-based regimen for stage I nonsmall cell lung cancer: a multicenter study. *Cancer* 2012; **118**: 2078–84. doi: <https://doi.org/10.1002/cncr.26470>
- Baumann P, Nyman J, Hoyer M, Wennberg B, Gagliardi G, Lax I, et al. Outcome in a prospective phase II trial of medically inoperable stage I non-small-cell lung cancer patients treated with stereotactic body radiotherapy. *J Clin Oncol* 2009; **27**: 3290–6. doi: <https://doi.org/10.1200/JCO.2008.21.5681>
- Fakiris AJ, McGarry RC, Yiannoutsos CT, Papiez L, Williams M, Henderson MA, et al. Stereotactic body radiation therapy for early-stage non-small-cell lung carcinoma: four-year results of a prospective phase II study. *Int J Radiat Oncol Biol Phys* 2009; **75**: 677–82. doi: <https://doi.org/10.1016/j.ijrobp.2008.11.042>
- Shultz DB, Trakul N, Abelson JA, Murphy JD, Maxim PG, Le QT, et al. Imaging features associated with disease progression after stereotactic ablative radiotherapy for stage I non-small-cell lung cancer. *Clin Lung Cancer* 2014; **15**: 294–301. doi: <https://doi.org/10.1016/j.clcc.2013.12.011>
- Davnull F, Yip CS, Ljungqvist G, Selmi M, Ng F, Sanghera B, et al. Assessment of tumor heterogeneity: an emerging imaging tool for clinical practice? *Insights Imaging* 2012; **3**: 573–89. doi: <https://doi.org/10.1007/s13244-012-0196-6>
- Yang X, Knopp MV. Quantifying tumor vascular heterogeneity with dynamic contrast-enhanced magnetic resonance imaging: a review. *J Biomed Biotechnol* 2011; **2011**: 732848: 1: 12. doi: <https://doi.org/10.1155/2011/732848>
- Asselin MC, O'Connor JP, Boellaard R, Thacker NA, Jackson A. Quantifying heterogeneity in human tumours using MRI and PET. *Eur J Cancer* 2012; **48**: 447–55. doi: <https://doi.org/10.1016/j.ejca.2011.12.025>
- Golden DI, Lipson JA, Telli ML, Ford JM, Rubin DL. Dynamic contrast-enhanced MRI-based biomarkers of therapeutic response in triple-negative breast cancer. *J*

- Am Med Inform Assoc* 2013; **20**: 1059–66. doi: <https://doi.org/10.1136/amiajnl-2012-001460>
16. Alic L, van Vliet M, van Dijke CF, Eggermont AM, Veenland JF, Niessen WJ. Heterogeneity in DCE-MRI parametric maps: a biomarker for treatment response? *Phys Med Biol* 2011; **56**: 1601–16. doi: <https://doi.org/10.1088/0031-9155/56/6/006>
 17. Alic L, Veenland J, van Vliet M, Van Dijke CF, Eggermont AM. Quantification of heterogeneity in dynamic contrast enhanced MRI data for tumor treatment assessment. *In Biomedical Imaging: Nano to Macro, 3rd IEEE International Symposium* 2006: 944–7.
 18. Mattonen SA, Palma DA, Haasbeek CJ, Senan S, Ward AD. Early prediction of lung cancer recurrence after stereotactic radiotherapy using second order texture statistics. *In Medical Imaging 2014: Biomedical Applications in Molecular, Structural, and Functional Imaging* 2014; **9038**.
 19. Johansen R, Jensen LR, Rydland J, Goa PE, Kvistad KA, Bathen TF, et al. Predicting survival and early clinical response to primary chemotherapy for patients with locally advanced breast cancer using DCE-MRI. *J Magn Reson Imaging* 2009; **29**: 1300–7. doi: <https://doi.org/10.1002/jmri.21778>
 20. Galbán CJ, Chenevert TL, Meyer CR, Tsien C, Lawrence TS, Hamstra DA, et al. The parametric response map is an imaging biomarker for early cancer treatment outcome. *Nat Med* 2009; **15**: 572–6. doi: <https://doi.org/10.1038/nm.1919>
 21. Unser M, Van De Ville D. Wavelet steerability and the higher-order Riesz transform. *IEEE Trans Image Process* 2010; **19**: 636–52. doi: <https://doi.org/10.1109/TIP.2009.2038832>
 22. Edge SB, Byrd DR, Compton CC, Fritz AG, Greene FL et al. eds. *AJCC cancer staging manual*, 7th ed. New York, NY; 2010 .
 23. Tibshirani R. The lasso method for variable selection in the Cox model. *Stat Med* 1997; **16**: 385–95. doi: [https://doi.org/10.1002/\(SICI\)1097-0258\(19970228\)16:4<385::AID-SIM380>3.0.CO;2-3](https://doi.org/10.1002/(SICI)1097-0258(19970228)16:4<385::AID-SIM380>3.0.CO;2-3)
 24. Chen W, Giger ML, Li H, Bick U, Newstead GM. Volumetric texture analysis of breast lesions on contrast-enhanced magnetic resonance images. *Magn Reson Med* 2007; **58**: 562–71. doi: <https://doi.org/10.1002/mrm.21347>
 25. Depeursinge A, Foncubierta-Rodriguez A, Van de Ville D, Müller H. Lung texture classification using locally-oriented Riesz components. *Med Image Comput Comput Assist Interv* 2011; **14**(Pt 3): pp. 231–238.
 26. Depeursinge A, Kurtz C, Beaulieu C, Napel S, Rubin D. Predicting visual semantic descriptive terms from radiological image data: preliminary results with liver lesions in CT. *IEEE Trans Med Imaging* 2014; **33**: 1669–76. doi: <https://doi.org/10.1109/TMI.2014.2321347>
 27. Harrington DP, Fleming TR. A class of rank test procedures for censored survival data. *Biometrika* 1982; **69**: 553–66. doi: <https://doi.org/10.1093/biomet/69.3.553>
 28. Bland JM, Altman DG. Survival probabilities (the Kaplan-Meier method). *BMJ* 1998; **317**: 1572.